



Human Journals

Review Article

October 2021 Vol.:13, Issue:1

© All rights are reserved by Shivani Deshmukh et al.

A Review on Role of Nanocarriers in Targeted Drug Delivery System



**Shivani Deshmukh*, Swati Nikam, A. B. velhal,
V.K. Redasani**

*YSPM's Yashoda Technical Campus, Faculty of
Pharmacy, Wadhe, Satara, India.*

Submitted: 23 September 2021

Accepted: 28 September 2021

Published: 30 October 2021



HUMAN JOURNALS

www.jcpr.humanjournals.com

Keywords: Nanoparticles, controlled release, novel drug delivery, targeted delivery, Nanomedicine

ABSTRACT

Over the last several decades, there's been a significant amount of exploration in the field of novel delivery as carriers for small to medium-size molecules. Particulate systems, such as nanoparticles, have been employed to change and improve the pharmacokinetic and pharmacodynamics aspects of a variety of pharmacological compounds. Nanocarriers have a lot of potential in the medical field. Nanoparticles in combination with medicinal substances overcome the deficiency of traditional therapy. Simple designed, functionalized liposomes, fullerenes, nanoparticles, hydrogels, micelles, dendrimers, and mesoporous particles have all been used effectively in the development of appropriate and nanocomposite drug delivery. Some issues, such as side effects and toxicity, are still being contested and should be thoroughly investigated before being used in biological systems. Our focus on the types of therapeutically employed nanocarriers and their therapeutic specificity, as well as their modern delivery systems for diseases such as cancer, infectious disease, autoimmune disease, cardiovascular disease, Alzheimer's disease, and Parkinson's disease. Nanomaterial provides remarkable advantages over the traditional drug delivery in terms of high stability, site-specificity, large drug-carrying capacity, and controlled release pattern, possibility to use in distinct route of administration, and the ability to conveyance hydrophilic and hydrophobic fragments. The purpose of this article is to demonstrate the potentiality of nanocarriers and their applications.

1. INTRODUCTION:

Recently advancement of novel methodologies for the development of nanoformulation to optimize medication offers a wide scope of biotechnology applications.

Nanocarriers provide the way to transport the drug to the objective site with decreased dose abundance in a controlled release manner to alleviate the adverse effect accomplished with conventional therapies. The consolidation of nanotechnology and pharmaceutical science is exponentially encouraging and has filled quickly in the recent past.

Nanoparticle ranges of 1-100nm. Biodegradable and stable NP carriers are suitable they are homoimmunogenic, simple to make cost-effective, and only release their payloads at the target spot [1].

Organic, inorganic, polymeric, and metallic nanostructures, some examples are 'dendrimers', 'micelles', 'solid lipid nanoparticles (SLNs)', 'carbon nanotubes', and 'liposomes', are frequently used as targeted and controlled drug delivery vehicles [2].

Low-soluble medicines with poor absorption properties, in particular, are enclosed with nanomaterial for controlled and long-term drug release. The effectiveness of these drug carriers, on the other hand, is determined by their size, shape, hydrophobicity, surface properties, and a variety of other chemical and biophysical characteristics [3, 4].

Regarding the possibility of nanocarriers in human disorders, this review will address a diversity of nanocarriers employed in chronic disease management.

2. Drug delivery system:

Drugs and other therapeutic agents are used to treat distinct diseases and conditions to deliver the intended pharmacological benefits with the least amount of adverse effects possible. The application of a controlled drug delivery pattern is a central strategy to raise the therapeutic adequacy and safety of therapeutic molecules [5, 6].

The ability to assure a higher and longer period of drug bioavailability, and hence better therapeutic efficacy, is the key rationale for selecting a suitable drug delivery method. The drug is conjugated with a variety of materials to make a nano-drug delivery system.

Targeted therapy is a method of treating disease that involves delivering small doses of a therapeutic agent to a specific part of the body over an extended length of time. To

accomplish this, one of the ultimate goals of nanomedicine is the production of safer and more effective therapeutic nanoparticles. A comprehensive explanation of promising drug delivery carriers is given below.

2.1 Nanoparticle:

As evidenced by a large amount of clinical and preclinical studies, the role of nanoparticles as therapeutic carriers has been thoroughly examined. Diverse hydrophilic and hydrophobic bricks of distinct structures, lengths, and charges have been used to prepare polymeric nanoparticles of various shapes, sizes, and stabilities. As a consequence, these nanoparticles may enclose and bind to hydrophilic and hydrophobic medicines, as well as macromolecules, such as proteins, antibodies, or nucleic acids [7].

Nanoparticles may also be invented to respond to foreign stimuli, including light, temperature, enzyme, pH, and other biological and chemical agents [8]. The conscience of amphiphilic copolymer chains in aqueous conditions is used to make polymeric nanoparticles [9]. These are of two categories organic and inorganic nanoparticles. Inorganic nanoparticles are assembled by various methods as 'Thermal decomposition' by 'crystallization of inorganic salt' and many more depend upon nanoparticles. Some examples of inorganic nanoparticles are GNPs, AgNPs, iron oxide, QDs, platinum, zinc oxide, ceramic oxide while liposomes, carbon nanomaterial, micelles, and dendrimers are organic nanoparticles. Nevertheless, Because of their great biocompatibility, polymeric nanoparticles are chosen over inorganic nanoparticles. a high degree of biodegradability, and reduced systemic adverse effect [10].

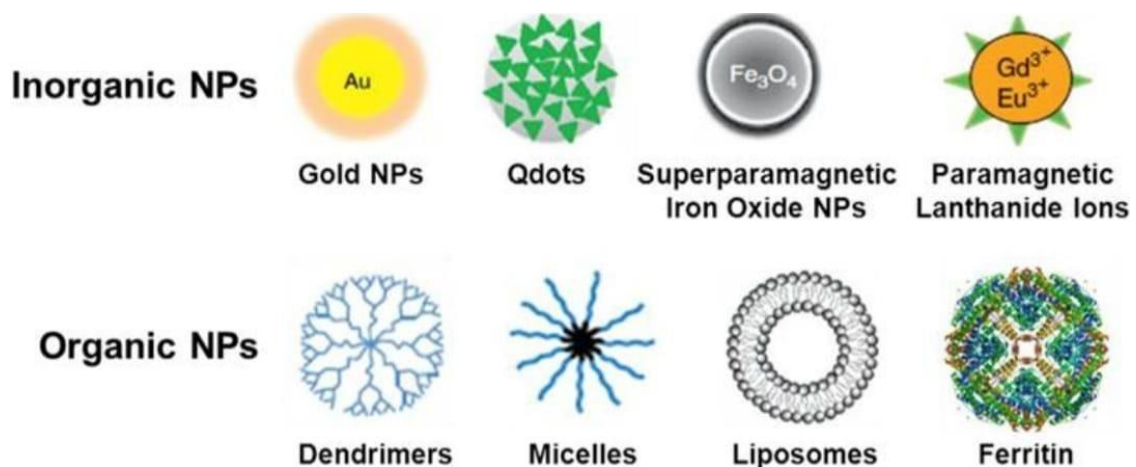


Fig No. 1: Organic and Inorganic nanoparticles [11].

Table No. 1: Depending upon dimension they were classified with example as follows:[11].

Elementary unit	Examples
0D Units(3 dimensions monometric range)	Molecules, Clusters, Fullerenes, metal carbides, powder, grains.
1D Units (2 dimensions monometric range)	Nanotubes, Fibres, filaments, whiskers, spirals, belts, springs, needles
2D Units (1 dimension monometric range)	Layers

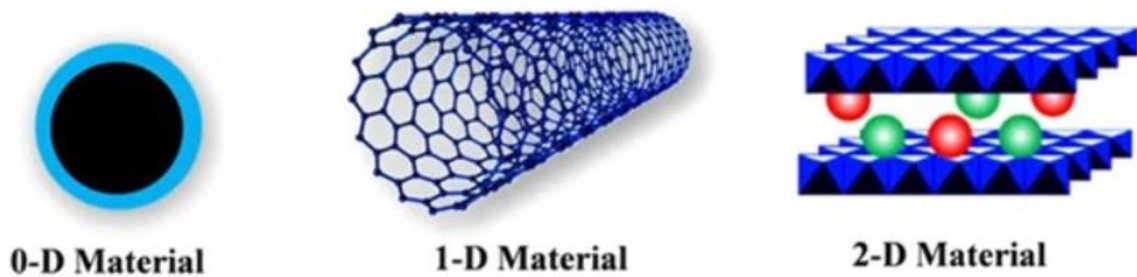


Fig No. 2: Classification according to dimensions [12].

2.2 Quantum Dots

Quantum dots (QDs) are tiny semiconducting particles or nanocrystals with dimensions ranging from 2 to 10 nm. These particles consist of a semiconductor inorganic core such as CdSe and an aqueous organic coated shell such as ZnS [13]. The QDs core structure determines colour emanate while its outer aqueous frame is used for conjugation of a biomolecule like a peptide, DNA, protein. QDs can also carry a cap, which improves their solubility in aqueous buffers. QDs can be utilized to track therapeutic drugs within cells/tissues because of their limited emission, strong fluorescence, and high photo-stability [14, 15].

2.3 Micelles

Micelles are formed due to the dispersion of amphiphilic molecules, consisting of a hydrophobic and hydrophilic constituent, in solution. The concentration of amphiphiles, the size of the hydrophobic/hydrophilic domains in the amphiphilic molecule, the temperature, and the solvent are all parameters that influence micelle formation [16]. Micelles are accessible to design as biodegradable and biocompatible allow systemic conveyance of

therapeutic agent to specific tissue. Polymeric micelles are mostly used for the systemic delivery of water-insoluble therapeutic agents. They are in < 100 nm size formed in solution as aggregate.

Micelles are self-build and proceed only when a certain minimum concentration is attained called critical micelle concentration. Polymer micelles are a promising way to target drugs due to their high stability, large drug loading capacity, and minimal cytotoxicity with the controlled and sustained pattern. Micelles are used in a variety of ways for targeted therapy, including the improved permeability and stimuli sensitivity, and ligand-based micelles, retention affect others. A drug is released upon internal stimuli (e.g., pH and enzyme) foreign stimuli (e.g., light and temperature) in a stimuli-sensitive method. . For example, a pH-sensitive micellar device could be utilized to transport drugs to tumors, that the tumor microenvironment has a somewhat acidic pH (-6.8) [17].

2.4 Hydrogel

Hydrogels, also known as hydrophilic gels, are polymeric systems that are physically or chemically bridged and have the ability to expand in the existence of water or organic solvents. Polar groups adhering to the polymeric backbone rely on their ability to soak water, while cross-linked polymeric matrix provides resistance to dissolution [18]. Hydrogel is prepared in many ways by single-step or multiple-step procedures. A single-step procedure includes the polymerization and parallels cross-linking of versatile monomers, although a multiple-step procedure employed the amalgamation of polymer molecules with reacting groups and their consequent cross-linking with convenient agents.

Hydrogels are biocompatible, non-toxic, and biodegradable with a large absorption capacity, which assures extensive biomedical applications in drug delivery, tissue engineering, and wound dressing/healing. Additionally, stimuli-responsive components such as pH and temperature-sensitive smart hydrogels hit site-specific drug delivery applications [19].

2.5 Liposomes

Liposomes are spherical vesicles synthesized through the hydration of dry phospholipids. They can be prepared in definite structure, composition, size, and plasticity with a range of lipid molecules and further surface modification. One of the most extensive advantages of liposomes is their capability to merge with the cell membrane and discharge their contentment into the cytoplasm, which makes them a convenient intelligent nanocarrier

method for targeted delivery. The simplest liposome is a collection of a lipid bilayer around a void core with a diameter of 50–1000 nm. The therapeutic molecules can be laden into this void core for transport [20]. Because of their biocompatibility, biodegradability, low toxicity, and site-specific transport of either hydrophilic or hydrophobic drugs, liposomes have gotten a lot of attention as drug delivery systems. The vesicle proportion and numerous bilayers determine the mass of encapsulated drug, and because of size, bilayer liposomes are split into two classes: multilamellar vesicles and unilamellar vesicles. Unilamellar vesicles can further be redevise as large unilamellar vesicles and small unilamellar vesicles. Unilamellar vesicles are a collection of a single phospholipid bilayer enclosing the aqueous mixture, whilst multilamellar vesicles are composed of coextensive phospholipid spheres detached by water layers [21]. At present, Stealth liposomes are currently favored above conventional liposomes because of their systemic stability and ability to avoid the mononuclear phagocytic system, which engulfs and removes liposomes from circulation (main topic). The liposomes are analyzed for the diversity of therapeutic applications, such as cancer diagnostic and management, vaccines, brain-specific drug delivery, and anti-microbial therapy [22].

2.6 Dendrimer

Dendrimers are globular, radially uniform, compact structures with tree-like arms and have high monodispersity. Branches of dendrimers are fabricated in very small sizes 1-5nm. The dendrimer structure consists of a central core composed of an atom or band of atoms from which branches of another atom called 'dendrons' grow through a series of chemical reactions[23]. Firstly dendrimers are synthesized by the convergent or divergent method. It is ideal drug vehicle that has diverse diagnostic and therapeutic applications due to its hyperbranched structure containing an elevated number of the functional group. Dendrimers possess free end clusters that can be easily changed to conjugate biocompatible chemicals, resulting in a molecule with minimal cytotoxicity and great bio-permeability. Surface changes can also be used to optimize therapeutic drug distribution to specific targets. Currently used mono or copolymer dendrimers are polyamidoamine (PAMAM), chitin, polyethyleneimine [24, 25].

2.7 Mesoporous material

Efficient drug loading and controlled release at the definite site can also be achieved by using the mesoporous component. Moreover, pore size, surface functionalization, and surface domain are the aim factors influencing drug loading and discharge behaviour[26]. There are

various methods by which mesoporous materials are prepared such as the sol-gel method, hydrothermal synthesis, microwave synthesis, and template synthesis[27]. By altering the reaction conditions, mesoporous materials with varied forms, sizes, and symmetries can be produced.

Mesoporous ceramics have been formulated by using several synthetic methods. At present, block copolymer preparation in acidic conditions is speedier (6–12 h) than typical methods (7 days). Moreover, modern processes such as microwave heating decreased the preparation time to lower than an hour together with control over the structure of the mesoporous ceramics [28].

2.8 Scaffold

The scaffolds in biomedicine and tissue engineering are essential because scaffolds assist cell adhesion, proliferation, and divergence for tissue expansion. Scaffold provides a porous system for the optimum expansion of cells, sometimes leading to the formation of tissue. The approach of using scaffolds is of enormous importance due to biocompatible biomaterial matrix is required for optimum cell expansion [29-31].

In tissue engineering, scaffolds are pattern offer structural support identical to that of naturally develop extracellular matrix. Scaffolds are working in the position of natural fibrous collagen throughout bone tissue engineering, which plays an essential role in bone restoration by regulating cell adherence, proliferation, and divergence [30].

Significantly, scaffolds provide key morphological and mechanical characteristics for clinical application, like high porosity, interconnectivity, and mechanical strength, together with high biocompatibility [31]. A few other methods are also implemented for the preparation of several forms of scaffolds, like rapid prototyping, bioprinting, stereolithography, fused deposition modeling, selective laser sintering [32].

2.9 Fullerenes

Fullerenes are carbon nanomaterial that can be complexed with a wide range of chemicals, allowing them to play an important role in science. Fullerenes have a crystalline molecular architecture and are organized in a soccer ball-like internal structure. Buckyballs, as they're also known, were developed in 1985 from the slag of laser vaporized graphite [33]. These carbon-based compounds have proven to be the most viable nanomaterials for diagnosing,

monitoring, and treating various medical diseases due to their unique structure and capabilities. In contrast to other compounds that could be used as cancer medication delivery channels, fullerenes do not break down in the body and are ingested whole. This property is useful for some cancer treatment chemicals that are harmful to healthy cells [34]. Fullerene can fit into HIV proteases' hydrophobic core. This reduces the accessibility of stimuli at the enzyme's catalytic site. It can also be utilized as an antioxidant and a radical scavenger [35].

3 Targeted Delivery Applications of Therapeutic Nanocarriers:

3.1 Nanoparticle targeting in cancer treatment:

Cancer, often known as malignant tumours, refers to a group of disorders in which uncontrolled cell development is caused by changes in the cell's genetic material. A high death rate, low quality of life, and expensive therapy are all consequences of cancer and its bad progenies for patients. Chemotherapy, injections of nanoparticles, radiation remedial treatment, and immunotherapy have all undergone significant technological progress and study in the fight against cancer. However, these technologies have some flaws associated with systemic distribution, such as low drug concentration at the tumor site, non-selectivity towards cells or tissues, which can contribute to toxicity, and low drug efficacy due to short half-lives.

The medicine is supplied directly to the desired place via implantation in local delivery systems. The fundamental benefit of local therapy is that the medicinal concentration of chemotherapeutics in the tumour environment can be increased while damage to nontargeted organs is reduced. Furthermore, local delivery can improve therapeutic efficacy by minimizing the prolonged way through a hostile territory that is required when the drug is transported systemically to the target site. Several carriers that can transport medications in a controlled manner without generating side effects have been investigated to better understand the tumour and boost drug availability. Since versatile materials like liposomes, polymer micelles, dendrimers, scaffolds, hydrogel, etc. have been employed to transport chemotherapeutic agents to a specific site to enhance the efficacy of the therapeutic drug.

Liposomes were the first nanocarriers to receive regulatory approval for transporting a variety of chemotherapeutic drugs [36, 37]. As previously stated, the Doxil was the first liposome formulation to be licensed on the market in 1995 for the management of Kaposi sarcoma related to AIDS. Other liposome forms for anticancer therapy, such as the DaunoXome®, are

also available to consumers [38]. Micelles have proven to be effective as hydrophobic drug haulers [39].

One example is the FDA's certification of Genexol-PM for the treatment of breast cancer [40]. The FDA granted the use of polymer nanoparticle albumin (Abraxane®) for chemotherapy transit in various types of cancer treatments [41]. Novel water-soluble and biocompatible dendritic systems have been developed using 2, 2-bis(hydroxymethyl)propanoic acid as a drug carrier for doxorubicin[42]. Zhong et al using polyamidoamine of version 4 and DOX via acid-sensitive hydrazone linkages, DOX conjugated dendrimers were created. These DOX conjugated dendrimers, when administered to mice bearing melanoma (B16-F10), reduced the tumor burden through enhanced accumulation and tumor penetration. Li and co-workers showed the size effect of pH-sensitive nanoparticles composed of dendrimer building blocks with better tumor penetration and their dissociation into smaller sizes in the tumor environment [43].

3.2 Nanoparticle targeting in Parkinson's disease:

Parkinson's disease (PD) is a neurodegenerative disease, which is caused by the dropping of dopaminergic neurons of the substantia nigra. This decrease in dopamine is correlated with motor impairment and eventually leads to tremor, bradykinesia, and rigidity [44].

Typically, patients are usually treated with dopamine agonists such as amantadine, budipine, and levodopa, but these medications have a poor benefit-to-side-effect ratio. The gold standard of treatment is still levodopa. The effectiveness of these medications wears off after a few years since the side effects make them unsuitable for long-term use. Furthermore, when it reaches the dopamine receptor, the bioavailability of orally taken medicines is influenced by some factors, including gastric pH and dietary protein. Other administration routes, such as intranasal, rectal, sublingual, or pulmonary, could not produce good results since any of them could keep the dopaminergic medication stimulated indefinitely. Nanoscale devise miniaturization and drug integration for continuous release have become key difficulties. Researchers are experimenting with dopamine-injected liposomes and investigating their efficiency in a rat model of Parkinson's disease. In a rat replica, dopamine conjugated on the surface of chitosan nanoparticles caused less harmful long-term release than dopamine alone. Aside from that, researchers have looked into polyethylene imine-grafted chitosan nanocarriers for gene delivery [45, 46].

Recently, a promising topic of interest for PD treatment has been L DOPA coated with manganese oxide, which can operate as a dual MRI contrast agent as well as a drug delivery agent [47]. Polymers such as polyvinyl pyrrolidone-poly (acrylic acid) (PVP/PAA) and polyvinyl pyrrolidone-poly (glycolic acid) (PLGA) have been used to synthesize NP, with animal studies revealing superior outcomes than free dopamine alone. In both the rat and monkey models, administration of a biodegradable nanoparticle to the PD-targeting compounds, which encompass neurotrophic elements such GDNF-MPs, resulted in superior structural and functional recovery of the Parkinsonian monkey.

3.3 Nanoparticle targeting in Alzheimer's disease:

Alzheimer's disease (AD) is among the most well-known neurodegenerative conditions affecting the elderly, with nearly incurable and restricted treatment options and unknown origins. One of the causes of nervous system degeneration, according to growing studies, is amyloid-beta ($A\beta$) overproduction and the inability of $A\beta$ peptides to be removed from the brain. Self-aggregation of this protein causes harmful oligomers, neurofibrillary plaques, and tangles to form as a sequel of its cumulative deposition [48].

The treatment of Alzheimer's disease using anti-medications of Alzheimer's is a very promising area of study, and several bioactive compounds have made it to clinical trials, but none have been successful. One of the main reasons for these failures is the drug's limited availability via the BBB. The cerebral microvascular endothelium, which bears various structural organizations of vascular beds, is anatomically described as the BBB. It has a limited number of alternative transport channels as well as tight cell-cell connections. The pinocytotic function is stopped, and the amount of intracellular fenestrae is greatly reduced. P glycoprotein, MDR Protein-I, and Breast Tumor Resistance Protein are among the active influx/efflux membrane transport proteins expressed by brain endothelial cells, as are other degradation enzymes that allow high selectivity of substances [49].

Therapeutic ceria (CeO_2) nanoparticles, which are potent and recyclable ROS scavengers that shuttle between Ce^{3+} and Ce^{4+} oxidation states, were recently explored by a group of researchers to see if they might eliminate ROS in mice genetically manipulated to show indications of Alzheimer's disease [50].

3.4 Nanoparticle targeting in diabetes mellitus:

Diabetes mellitus is a category of metabolic disorders discriminated by high blood glucose in the bloodstream due to dropped insulin binding effectiveness on cell surface receptors or decreased insulin release by cells. Type 1 diabetes is a sequel to the inadequacy of β cells that are demolished by the immune structure. Type 2 diabetes is chiefly involved with β cell dysfunction and insulin resistance. Both type 1 and 2 diabetes share common characteristics, i.e., β cell mass reduction [51].

Self-monitoring of insulin injections and blood glucose levels is amongst the most difficult aspects of diabetes care. With carbon nanotubes, glucose nanosensors, QDs, nano pumps, oral insulin, microspheres, and artificial pancreas, nanomedicine has added a new dimension to diabetes treatment. Because glucose nanosensors are used in implanted devices, monitoring and instantaneous tracking of blood glucose levels can be more accurate. This could potentially serve as a foundation for glucose-receptive nanoparticles that superiorly replicate the body's physiological insulin demands. The electrostatic charge of random layers of positively and negatively charged polymers is connected with the layer-by-layer approach.

The polymers are made into tiny films with pore sizes that are customizable, biocompatible, and flexible. As a "smart tattoo," these bilayers might well be permanently placed in subcutaneous tissue. Semi-permeable capsules, contrarily, allow glucose to pass through the interstitial fluid while safeguarding the sensor. Insulin is delivered through biodegradable polymeric carriers with a matrix encased in a nanoporous laminate containing grafted glucose oxidase. The surrounding nanoporous membrane changes when blood glucose levels rise, inducing biodegradation and, as a result, insulin transport. The glucose/glucose oxidase process lowers the pH in the microenvironment of the delivery mechanism. This causes the polymer system to swell, resulting in increased insulin release [52].

3.5 Nanoparticle targeting in cardiovascular diseases:

Cardiovascular diseases (CVDs) are a leading source of morbidity and fatality throughout the world. Although an immense number of treatment medicines are available in the cardiovascular era, their capacity to permeate the target tissue has hampered their effectiveness. Nanomaterial, contrastingly, avoid fast renal elimination and remain in circulation for a longer interval. This property enhances extravasation through the circulatory

system, allowing nanomaterial to accumulate and distribute effectively in the desired tissue or organs, resulting in optimum therapeutic efficacy with the smallest drug dosage.

Blood pressure

The most widely utilized nanomedicine at the moment is FDA-approved polymeric nanocarriers coupled to standard pharmaceuticals for enhanced absorption and bioavailability. pH-sensitive medications can be delivered via polymeric nanoparticles such as PLGA, PCL, eudragit, and chitosan [53]. Polymer-based nisoldipine eudragit \$100 nanoparticles released the drug from the polymer at the pH of the colon, potentially bypassing metabolic alterations in the gut and liver and prolonging the drug's bioavailability in blood circulation [54]. Furthermore, because of the higher solubility and bioavailability of felodipine (calcium-channel blocker) encapsulated in PLGA NPS, the drug's antihypertensive effects were improved [55]. When other regularly used hypertension medications (hydrochlorothiazide, amlodipine, and candesartan) were conjoined with PLGA NP5, similar results were obtained [56].

Another intriguing way to regulate BP is nanoparticle-mediated gene inactivation, which works primarily via siRNA-mediated gene expression regulation. As a result, siRNA is very susceptible to degradation and necessitates the use of a delivery channel to avoid deterioration by endo- and exonucleases found in the bloodstream and cells [57].

Cyclodextrin NPs are also recognized as effective drug transporters, and the hydrophobic core of cyclodextrins prevents the medication from degradation, extending its bioavailability. Mariangela et al. found that encapsulating captopril in cyclodextrin nanoparticles reduced blood pressure significantly, especially at lower doses [58].

3.6 Nanoparticles in Autoimmune Diseases:

The two most common diseases treated with nano-delivery systems are rheumatoid arthritis (RA) and acquired immunodeficiency syndrome (AIDS). RA is a prevalent and severe autoimmune disease that acts on nearly 1% of the comprehensive population. Even though the etiology is unknown, the bone and cartilage degradation is most likely caused by a complicated interaction between immune mediators. New therapy approaches can improve a patient's quality of life; however, a limited administration route and the need for repeated long-term treatment can cause systemic side effects.

Nanoparticle systems have the potential to deliver therapeutic medicines to inflamed tissue (synovial membrane) while avoiding systemic and unwanted side effects. TNF- α inhibitor certolizumab pegol (CZP) is commonly utilized in the clinic [59]. CZP nano-formulation with PEG extends its half-life to 14 days, and clinical studies on RA patients have shown promising outcomes for long-term treatment [60]. Using stand-alone C60 fullerenes (non-drug loaded) to target inflammatory tissues demonstrated promising outcomes in RA management by lowering synovitis and alleviating bone resorption and destruction [61].

AIDS is another autoimmune disorder lacking treatment. At present, clinical therapy is called highly active antiretroviral treatment (HAART), which comprises a combination of at minimum three anti-HIV medications repressing HIV replication. Despite this therapeutic path having contributed to a reduced mortality rate, it is not wholly effective [62].

Nano-delivery systems based on polymeric and liposomal nano-carriers have recently been developed to give a target-specific and sustained release formulation of anti-HIV medicines. The goal is to improve anti-HIV treatment efficacy while limiting systemic negative effects [63]. Efavirenz is loaded into poly (propylene imine) dendrimers (TUPPI) that are adorned with Tuftsin, for example. Tuftsin allowed final TuPPI particles to detect mononuclear phagocytic cells, resulting in considerably greater absorption in HIV-infected macrophages than uninfected cells [64].

CONCLUSION:

Nanotechnology is projected to revolutionize manufacturing over the coming years and will have a huge impact on life sciences, such as drug delivery, diagnostics, and biomaterial synthesis. In the realm of biomedical research, the development of targeted drug delivery systems that alter the distribution, absorption, and pharmacokinetics of medicinal drugs is vital. The ability of nanoparticles to transform low soluble, poorly absorbed, and labile biologically active substances into viable deliverable medications has huge potential. During the last decade, the use of nanomedicines has increased at an unparalleled rate. The desire to boost present treatments, site-specific delivery, and eventually better patient compliance are all reasons for creating nanotechnology-based drugs. Nanomedicines have several advantages over traditional treatments, including reduced toxicity and increased efficacy due to controlled drug release and enhanced pharmacokinetics and pharmacodynamics. To achieve site-specific, long-term drug administration, an appropriate drug carrier is required.

Nanotechnology focuses on the very small, making it ideal for developing systems that precisely administer medications to small parts of the body.

Because nanotechnology is the most potential area for diagnosis and treatment, more clinical trials from all over the globe are required. Nanotechnology-enabled medication delivery also allows pharmaceuticals to pass through cell membranes, which is crucial for the predicted expansion of genetic medicine in the next years. Nanomedicine is the way of the future, and nanoparticle-based therapies are at the center of it. To develop the notion of nanoparticle technology into a viable application as the next generation of medication delivery systems, more progress is required.

ACKNOWLEDGMENT:

The author intended to express their sincere thanks to the Honourable principal and professors of Yashoda Technical Campus, Faculty of Pharmacy, (Wadhe) Satara for motivating and inspiring to write this futuristic article.

REFERENCES:

1. G. Poste and R. Kirsh, "Site-specific (targeted) drug delivery in cancer therapy," *Bio/Technology*, 1983 vol. 1, no. 10, pp. 869–878.
2. Lombardo, D., Kiselev, M. A. & Caccamo, M. T. Smart nanoparticles for drug delivery application: development of versatile nanocarrier platforms in biotechnology and nanomedicine. *J. Nanomater* .2019, 3702518.
3. Patel, D. K. et al. Influence of graphene on self-assembly of polyurethane and evaluation of its biomedical properties. *Polymer* 65, 2015; 183–192.
4. Senapati, S., Mahanta, A. K., Kumar, S. & Maiti, P. Controlled drug delivery vehicles for cancer treatment and their performance. *Signal Transduct. Target.*2018 Ther. 3, 7.
5. Patel, D. K. et al. Functionalized graphene tagged polyurethanes for corrosion inhibitor and sustained drug delivery. *ACS Biomater. Sci. Eng.*2017; 3, 3351–3363.
6. Mahanta, A. K. et al. Polyurethane-grafted chitosan as new biomaterials for controlled drug delivery. *Macromolecules* 2015; 48, 2654–2666.
7. Elsabahy, M. & Wooley, K. L. Design of polymeric nanoparticles for biomedical delivery applications. *Chem. Soc. Rev* 2012; 41, 2545–2561.
8. Wang, Y., Shim, M. S., Levinson, N. S., Sung, H. W. & Xia, Y. Stimuli-responsive materials for controlled release of theranostic agents. *Adv. Funct. Mater.*2014; 24, 4206–4220.
9. Park, W. & Na, K. Advances in the synthesis and application of nanoparticles for drug delivery. *Wiley Interdiscip. Rev. Nanomed. Nanobiotechnology* 2015; 7, 494–508.
10. Anselmo, A. C. & Mitragotri, S. A review of clinical translation of inorganic nanoparticles. *AAPS J.* 201517, 1041–1054.
11. AnbazhaganMageswari, Ramachandrsn Srinivasan, Parthiban Subramanian, Nachimuthu Ramesh, *Nanomaterials: Classification, Biological Synthesis and Characterization | SpringerLink*
12. Akhand Pratap Singh , Arpan Biswas , Aparna Shukla1 and Pralay Maiti"Targeted therapy in chronic diseases using nanomaterial-based drug delivery vehicles*Signal Transduction and Targeted Therapy"* 2019;3-15
13. Iga, A.M.; Robertson, J.H.; Winslet, M.C.; Seifalian, A.M. Clinical potential of quantum dots. *J. Biomed. Biotechnol.* 2007, 76087.

14. Matea, C.T.; Mocan, T.; Tabaran, F.; Pop, T.; Mosteanu, O.; Puia, C.; Iancu, C.; Mocan, L. Quantum dots in imaging, drug delivery and sensor applications. *Int. J. Nanomed.* 2017, 12, 5421–5431.
15. Bailey, R.E.; Smith, A.M.; Nie, S. Quantum dots in biology and medicine. *Phys. E Low-Dimens. Syst. Nanostructures* 2004, 25, 1–12.
16. Gaucher, G. et al. Block copolymer micelles: preparation, characterization and application in drug delivery. *J. Control. Release* 2005; 109, 169–188.
17. Bae, Y., Fukushima, S., Harada, A. & Kataoka, K. Design of environment-sensitive supramolecular assemblies for intracellular drug delivery: Polymeric micelles that are responsive to intracellular pH change. *Angew. Chem. Int. Ed.* 2003; 42, 4640–4643.
18. Ahmed, E. M. Hydrogel: Preparation, characterization, and applications: a review. *J. Adv. Res.* 2015; 6, 105–121.
19. Hoffman, A. S. Hydrogels for biomedical applications. *Adv. Drug Deliv. Rev* 2012; 64, 18–23.
20. Leucuta, S.E. Nanotechnology for delivery of drugs and biomedical applications. *Curr. Clin. Pharm.* 2010, 5, 257–280.
21. Sharma, A. & Sharma, U. S. Liposomes in drug delivery: progress and limitations. *Int. J. Pharm.* 1997; 154, 123–140.
22. Daraee, H.; Etemadi, A.; Kouhi, M.; Alimirzalu, S.; Akbarzadeh, A. Application of liposomes in medicine and drug delivery. *Artif. Cells Nanomed. Biotechnol.* 2016, 44, 381–391.
23. Abbasi, E. et al. Dendrimers: synthesis, applications, and properties. *Nanoscale Res. Lett.* 2014; 9, 247.
24. Hsu, H.J.; Bugno, J.; Lee, S.R.; Hong, S. Dendrimer-based nanocarriers: A versatile platform for drug delivery. *Wiley Interdiscip Rev. Nanomed. Nanobiotechnol.* 2017, 9, 1–21.
25. Palmerston Mendes, L.; Pan, J.; Torchilin, V.P. Dendrimers as Nanocarriers for Nucleic Acid and Drug Delivery in Cancer Therapy. *Molecules* 2017, 22, 1401.
26. Manzano, M. & Vallet-Regí, M. New developments in ordered mesoporous materials for drug delivery. *J. Mater. Chem.* 2010; 20, 5593–5604.
27. Zhao, P. et al. Synthesis and drug delivery applications for mesoporous silica nanoparticles. *J. Med. Biotechnol.* 2017; 1, 1–8.
28. Yu, C., Fan, J., Tian, B., Stucky, G. D. & Zhao, D. Synthesis of mesoporous silica from commercial poly (ethylene oxide)/poly (butylene oxide) copolymers: toward the rational design of ordered mesoporous materials. *J. Phys. Chem. B* 2003; 107, 13368–13375.
29. Biswas, A., Amarajeewa, M., Senapati, S., Sahu, M. & Maiti, P. Sustained release of herbal drugs using biodegradable scaffold for faster wound healing and better patient compliance. *Nanomedicine* 2018; 14, 2131–2141.
30. Ma, P. X. & Zhang, R. Synthetic nano-scale fibrous extracellular matrix. *J. Biomed. Mater. Res.* 1999; 46, 60–72.
31. Smith, I., Liu, X., Smith, L. & Ma, P. Nanostructured polymer scaffolds for tissue engineering and regenerative medicine. *Wiley Interdiscip. Rev. Nanomed. Nanobiotechnology* 2009; 1, 226–236.
32. Eltom, A., Zhong, G. & Muhammad, A. Scaffold techniques and designs in tissue engineering functions and purposes: a review. *Adv. Mater. Sci. Eng.* 2019, 3429527.
33. Jiang, W., Kim, B.Y.S., Rutka, J.T., Chan, W.C.W.: Advances and challenges of nanotechnology-based drug delivery systems. *Expert Opin. Drug Deliv.* 2007; 4(6), 621–633.
34. Chan, W.C.W.: *Bio-applications of Nanoparticles*, vol. 620. Springer Science and Business Media (2009)
35. Bakry, R., Vallant, R.M., Najam-ul-Haq, M., Rainer, M., Szabo, Z., Huck, C.W., Bonn, G.N.K.: Medicinal applications of fullerenes. *Int. J. Nanomed.* 2007; 2(4), 639.
36. Gabizon AA. Stealth liposomes and tumor targeting: one step further in the quest for the magic bullet. *Clin Cancer Res.* 2001; 7(2):223-5.
37. Safra T, Muggia F, Jeffers S, Tsao-Wei DD, Groshen S, Lyass O, et al. Pegylated liposomal doxorubicin (doxil): reduced clinical cardiotoxicity in patients reaching or exceeding cumulative doses of 500 mg/m². *Ann Oncol.* 2000; 11(8):1029-33.
38. Presant CA, Scolaro M, Kennedy P, Blayney DW, Flanagan B, Lisak J, et al. Liposomal daunorubicin treatment of HIV-associated Kaposi's sarcoma. *Lancet.* 1993; 341(8855):1242-3.

39. Jhaveri AM, Torchilin VP. Multifunctional polymeric micelles for delivery of drugs and siRNA. *Front Pharmacol.* 2014; 5(77):1-26.
40. Oerlemans C, Bult W, Bos M, Storm G, Nijsen JF, Hennink WE. Polymeric micelles in anticancer therapy: targeting, imaging and triggered release. *Pharm Res.* 2010; 27(12):2569-89. Review
41. Gradishar WJ. Albumin-bound paclitaxel: a next-generation taxane. *Expert Opin Pharmacother.* 2006;7(8):1041-53. Review
42. Jesús, PadillaDe, Ihre, O. L., Gagne, H. R., Fréchet, L., Szoka, J. M. J. & Polyester, F. C. Dendritic systems for drug delivery applications: in vitro and in vivo evaluation. *Bioconjugate Chem.* 2002; 13, 453–461.
43. Li, H.-J. et al. Smart superstructures with ultrahigh pH-sensitivity for targeting acidic tumor microenvironment: instantaneous size switching and improved tumor penetration. *ACS nano* 2016;10, 6753–6761.
44. Dinda, S.C., Pattnaik, G.: Nanobiotechnology-based drug delivery in brain targeting. *Curr. Pharm. Biotechnol.* 14(15), 1264–1274 (2013)
45. Gendelman, H.E., Anantharam, V., Bronich, T., Ghaisas, S., Jin, H., Kanthasamy, A.G., Liu, X., McMillan, J., Mosley, R.L., Narasimhan, B.: Nanoneuromedicines for degenerative, inflammatory, and infectious nervous system diseases. *Nanomed. Nanotechnol. Biol. Med.* 2015;11(3), 751–767.
46. Lu, H., Dai, Y., Lv, L., Zhao, H.: Chitosan-graft-polyethyleneimine/DNA nanoparticles as novel non-viral gene delivery vectors targeting osteoarthritis. *PLoS ONE* 9(1), e84703 (2014)
47. McDonagh, B.H.: Multifunctional nanoparticles for bioimaging (2015)
48. Robinson, M., Lee, B.Y., Leonenko, Z.: Drugs and drug delivery systems targeting amyloid-b in Alzheimer's. *AIMS Mol. Sci.* 2015; 2(3), 332–358.
49. Pahnke, J., Wolkenhauer, O., Krohn, M., Walker, L.C.: Clinicopathologic function of cerebral ABC transporters implications for the pathogenesis of Alzheimer's disease. *Curr. Alzheimer Res.* 2008; 5(4), 396.
50. Kwon, H.J., Cha, M.-Y., Kim, D., Kim, D.K., Soh, M., Shin, K., Hyeon, T., Mook-Jung, I.: Mitochondria-targeting ceria nanoparticles as antioxidants for Alzheimer's disease. *ACS Nano* 2016; 10(2), 2860–2870.
51. Matveyenko, A.V., Butler, P.C.: Relationship between b-cell mass and diabetes onset. *Diabetes Obes. Metab.* 2008; 10(s4), 23–31.
52. Anindita Chowdhury¹, Selvaraj Kunjiappan, Theivendren Panneerselvam, Balasubramanian Somasundaram, Chiranjib Bhattacharjee Nanotechnology and nanocarrier-based approaches on treatment of degenerative diseases.(2017)
53. Desai, P. P., Date, A. A. & Patravale, V. B. Overcoming poor oral bioavailability using nanoparticle formulations—opportunities and limitations. *Drug Discov. Today. Technol.* 2012; 9, e87–e95.
54. Nepolean, R., Narayanan, N., Subramaniam, N., Venkateswaran, K. & Vinoth, J. Colon targeted methacrylic acid copolymeric nanoparticles for improved oral bioavailability of nisoldipine. *Int. J. Biol. Pharm. Res.* 2012;3, 962–967.
55. Shah, U., Joshi, G. & Sawant, K. Improvement in antihypertensive and antianginal effects of felodipine by enhanced absorption from PLGA nanoparticles optimized by factorial design. *Mater. Sci. Eng.: C.* 2014; 35, 153–163.
56. Arora, A. et al. Development of sustained release “nanofdc (fixed dose combination)” for hypertension—an experimental study. *PLoS ONE* 10, e0128208 (2015).
57. Nolte, A., Schneider, M., Walker, T. & Wendel, H. in *Regenerative Medicine and Tissue Engineering-Cells and Biomaterials* (IntechOpen, 2011).
58. Mariangela de Burgos, Md et al. New formulation of an old drug in hypertension treatment: the sustained release of captopril from cyclodextrin nanoparticles. *Int. J. Nanomed.* 6, 1005 (2011).
59. Gu, H.; Ho, P.L.; Tsang, K.W.; Wang, L.; Xu, B. Using biofunctional magnetic nanoparticles to capture vancomycin-resistant enterococci and other gram-positive bacteria at ultralow concentration. *J. Am. Chem. Soc.* 2003, 125, 15702–15703.
60. Horton, S.; Walsh, C.; Emery, P. Certolizumab pegol for the treatment of rheumatoid arthritis. *Expert Opin. Biol.* 2012, 12, 235–249.
61. Yudoh, K.; Karasawa, R.; Masuko, K.; Kato, T. Water-soluble fullerene (C60) inhibits the development of arthritis in the rat model of arthritis. *Int. J. Nanomed.* 2009, 4, 217–225.

62. de Castro, S.; Camarasa, M.J. Polypharmacology in HIV inhibition: Can a drug with simultaneous action against two relevant targets be an alternative to combination therapy? *Eur. J. Med. Chem.* 2018, 150, 206–227.
63. Herskovitz, J.; Gendelman, H.E. HIV and the Macrophage: From Cell Reservoirs to Drug Delivery to Viral Eradication. *J. Neuroimmune Pharm.* 2019, 14, 52–67.
64. Dutta, T.; Garg, M.; Jain, N.K. Targeting of efavirenz loaded tuftsin conjugated poly(propyleneimine) dendrimers to HIV infected macrophages in vitro. *Eur. J. Pharm. Sci.* 2008, 34, 181–189.

